# Package 'fMRIscrub'

October 25, 2023

```
Type Package
Title Scrubbing and Other Data Cleaning Routines for fMRI
Version 0.14.5
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Description Data-driven fMRI denoising with projection scrubbing (Pham et al
      (2022) <doi:10.1016/j.neuroimage.2023.119972>). Also includes routines for
      DVARS (Derivatives VARianceS) (Afyouni and Nichols (2018)
      <doi:10.1016/j.neuroimage.2017.12.098>), motion scrubbing (Power et al
      (2012) <doi:10.1016/j.neuroimage.2011.10.018>), aCompCor (anatomical
      Components Correction) (Muschelli et al (2014)
      <doi:10.1016/j.neuroimage.2014.03.028>), detrending, and nuisance
      regression. Projection scrubbing is also applicable to other
      outlier detection tasks involving high-dimensional data.
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# Description

Visualize artifact patterns from the results of pscrub. Requires pscrub(..., get\_dirs=TRUE).

# Usage

```
artifact_images(psx, idx = NULL, use_dt = TRUE)
```

# Arguments

psx	A "scrub_projection" object containing projection scrubbing results.
idx	The timepoints or column indexes for which to compute artifact images. If NULL (default), use the outlying timepoints.
use_dt	If detrended components are available (the "U" matrix of PCA or "M" matrix of ICA), should they be used to compute the artifact images? Otherwise, use the non-detrended components. Default: TRUE.

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#### **Details**

Computes two types: "mean" artifact images based on a weighted sum of the projection directions, with weights determined by the scores for each component at the flagged timepoint, and "top" artifact images based on the projection direction with the greatest score at the flagged timepoint.

#### Value

A list of three: idx, the timepoints for which the artifact images were computed; mean, the "mean" artifact images; and top, the "top" artifact images. The row names of the top artifact images matrix give the index of the top component ("V" in PCA and "S" in ICA) at each timepoint.

Dat1

First Example Time Series from the ABIDE

# Description

A sagittal slice from the fMRI time series for subject 0050048. The scan was obtained at the University of Pittsburgh School of Medicine. The scan has been pre-processed with slice time correction, rigid body realignment estimation, spatial normalization to MNI space, and linear detrending. Subject 0050048 was a typically-developing 11-year-old male. The scan has many artifacts. A mask was applied to vectorize the spatial dimensions.

## Usage

Dat1

## Format

A numeric matrix of 193 time points by 4675 voxels

#### **Details**

Source: http://fcon\_1000.projects.nitrc.org/indi/abide/abide\_I.html

## References

• 1.Di Martino, A. et al. The autism brain imaging data exchange: towards a large-scale evaluation of the intrinsic brain architecture in autism. Mol Psychiatry 19, 659–667 (2014).

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Dat2

Second Example Time Series from the ABIDE

#### **Description**

A sagittal slice from the fMRI time series for subject 0051479. The scan was obtained at the California Institute of Technology. The scan has been pre-processed with slice time correction, rigid body realignment estimation, spatial normalization to MNI space, and linear detrending. Subject 0051479 was a typically-developing 20-year-old female. The scan has few visible artifacts. A mask was applied to vectorize the spatial dimensions.

# Usage

Dat2

#### **Format**

A numeric matrix of 145 time points by 4679 voxels

#### **Details**

Source: http://fcon\_1000.projects.nitrc.org/indi/abide/abide\_I.html

#### References

• 1.Di Martino, A. et al. The autism brain imaging data exchange: towards a large-scale evaluation of the intrinsic brain architecture in autism. Mol Psychiatry 19, 659–667 (2014).

**DVARS** 

**DVARS** 

# **Description**

Computes the DSE decomposition and DVARS-related statistics. Based on code from github.com/asoroosh/DVARS

```
DVARS(
   X,
   normalize = TRUE,
   cutoff_DPD = 5,
   cutoff_ZD = qnorm(1 - 0.05/nrow(as.matrix_ifti(X))),
   verbose = FALSE
)
```

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# **Arguments**

Χ

a T by N numeric matrix representing an fMRI run. There should not be any missing data (NA or NaN).

normalize

Normalize the data? Default: TRUE. Normalization removes constant-zero voxels, scales by 100 / the median of the mean image, and then centers each voxel on its mean.

To replicate Afyouni and Nichols' procedure for the HCP MPP data, since the HCP scans are already normalized to 10,000, just divide the data by 100 and center the voxels on their means:

Y <- Y/100; DVARS(t(Y - apply(Y, 1, mean))) where Y is the V by T data matrix

Note that while voxel centering doesn't affect DVARS, it does affect DPD and ZD.

cutoff\_DPD, cutoff\_ZD

Numeric outlier cutoffs. Timepoints exceeding these cutoffs will be flagged as

verbose

Should occasional updates be printed? Default is FALSE.

#### Value

A list with components

**measure** A data frame with T rows, each column being a different variant of DVARS.

measure info "DVARS"

**outlier\_cutoff** The outlier cutoff value(s).

**outlier\_flag** A logical data frame with T rows, where TRUE indicates suspected outlier presence.

#### References

Afyouni, S. & Nichols, T. E. Insight and inference for DVARS. NeuroImage 172, 291-312 (2018).

FD

Framewise Displacement

# **Description**

Calculate Framewise Displacement (FD)

6 FD

## Usage

```
FD(
    X,
    trans_units = c("mm", "cm", "in"),
    rot_units = c("deg", "rad", "mm", "cm", "in"),
    brain_radius = NULL,
    detrend = FALSE,
    lag = 1,
    cutoff = 0.3
)
```

#### **Arguments**

)	(	An I	V b	y 6	matrix	in	which	the	first	three	columns	represent	the	transl	ational	

RPs (trans\_units), and the second three columns represent the rotational RPs (rot\_units). If rot\_units measures an angle, it will be converted to trans\_units by measuring displacement on a sphere of radius brain\_radius trans\_units. Alternatively, this can be the file path to an N by 6 matrix which can be read

with read. table (fields separated by white-space; no header).

trans\_units "mm" for millimeters (default), "cm" for centimeters, or "in" for inches.

rot\_units "deg" for degrees (default), "rad" for radians, or one of the trans\_units op-

tions.

brain\_radius If rot\_units measures an angle, the rotational RPs are transformed to a spatial

measurement representing the displacement on a sphere of radius brain\_radius

trans\_units.

If brain\_radius is NULL (default), it will be set to 50 mm.

detrend Detrend each RP with the DCT before computing FD? Default: FALSE. Can be

a number of DCT bases to use, or TRUE to use 4.

lag The difference of indices between which to calculate change in position. De-

fault: 1 (the previous timepoint). Changing this argument sets  $\Delta x_i = x_{i-lag}$  –

 $x_i$  (and similarly for the other RPs).

cutoff FD values higher than this will be flagged. Default: .3.

#### **Details**

The FD formula is taken from Power et. al. (2012):

$$FD_i = |\Delta x_i| + |\Delta y_i| + |\Delta z_i| + |\Delta \alpha_i| + |\Delta \beta_i| + |\Delta \gamma_i|$$

where i is the timepoint; x, y and z are the translational realignment parameters (RPs);  $\alpha$ ,  $\beta$  and  $\gamma$  are the rotational RPs; and  $\Delta x_i = x_{i-1} - x_i$  (and similarly for the other RPs).

#### Value

A list with components

**measure** A length N vector of FD values in trans\_units.

flags\_to\_nuis\_spikes 7

```
measure_info "FD"

outlier_cutoff cutoff

outlier_flag A length-N logical vector, where TRUE indicates suspected outlier presence.
```

#### References

• Power, J. D., Barnes, K. A., Snyder, A. Z., Schlaggar, B. L. & Petersen, S. E. Spurious but systematic correlations in functional connectivity MRI networks arise from subject motion. Neuroimage 59, 2142-2154 (2012).

flags\_to\_nuis\_spikes Flags to nuisance spikes

# **Description**

Convert flagged volumes to corresponding one-hot encoded vectors which can be used for nuisance regression.

## Usage

```
flags_to_nuis_spikes(flags, n_time)
```

# **Arguments**

flags	Numeric vector of integers indicating the indices of the flagged volumes. Or, a logical vector of length n_time where TRUE values indicate the flagged volumes.
n_time	The length of the vectors to obtain. For nuisance regression, this is the length of the BOLD data. The highest index in flags should not exceed n_time.

# Value

A numeric matrix of ones and zeroes. The number of rows will be n\_time and the number of columns will be the number of flags. Each column will have a 1 at the flag index, and 0 elsewhere.

fMRIscrub: fMRIscrub: fMRI scrubbing and other data cleaning routines

## **Description**

See help(package="fMRIscrub") for a list of functions.

8 leverage

#### **Description**

The kurtosis cutoff is a high quantile (default 0.99) of the sampling distribution of kurtosis for Normal iid data of the same length as the components; it is estimated by simulation or calculated from the theoretical asymptotic distribution if the components are long enough.

## Usage

```
high_kurtosis(Comps, kurt_quantile = 0.99, n_sim = 5000, min_1 = FALSE)
```

#### **Arguments**

Comps	A matrix; each column is a component. For PCA, this is the U matrix. For ICA, this is the M matrix.
kurt_quantile	components with kurtosis of at least this quantile are kept.
n_sim	The number of simulation data to use for estimating the sampling distribution of kurtosis. Only used if a new simulation is performed. (If $n < 1000$ and the quantile is 90%, a pre-computed value is used instead. If $n > 1000$ , the theoretical asymptotic distribution is used instead.)
min_1	Require at least one component to be selected? In other words, if no components meet the quantile cutoff, should the component with the highest kurtosis be returned? Default: FALSE.

## **Details**

The components should not have any strong low-frequency trends, because trends can affect kurtosis in unpredictable ways unrelated to outlier presence.

# Value

A logical vector indicating whether each component has high kurtosis.

# Description

Computes the leverage of each observation in the PC score (U) or IC mixing (M) matrix for projection scrubbing. Can threshold to flag potential outliers.

```
leverage(Comps, are_norm = FALSE, median_cutoff = NULL)
```

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#### **Arguments**

Comps The n by Q PC score matrix/IC mixing matrix.

are\_norm Assume the columns of Comps are orthogonal and have 2-norms equal to 1?

Speeds up the computation.

median\_cutoff The outlier cutoff, in multiples of the median leverage. Default: NULL (do not

compute outliers).

# Value

A list with entries "meas" (the leverage values), "cut" (the leverage cutoff value) and "flag" (logical vector indicating the outliers). If !is.null(median\_cutoff), "cut" and "flag" are omitted.

plot.scrub\_DVARS

Plot a "scrub\_DVARS" object

# **Description**

```
Plot a "scrub_DVARS" object
```

## Usage

```
## S3 method for class 'scrub_DVARS'
plot(x, title = NULL, ...)
```

#### **Arguments**

x The "scrub\_DVARS" object

title (Optional) If provided, will add a title to the plot.

... Additional arguments to ggplot, e.g. main, sub, xlab, ylab, legend.position

# Value

A ggplot

plot.scrub\_FD

Plot a "scrub\_FD" object

# **Description**

```
Plot a "scrub_FD" object
```

# Usage

```
## S3 method for class 'scrub_FD'
plot(x, title = NULL, ...)
```

# Arguments

x The "scrub\_FD" object

title (Optional) If provided, will add a title to the plot.

... Additional arguments to ggplot, e.g. main, sub, xlab, ylab, legend.position

# Value

A ggplot

```
\verb"plot.scrub_projection" \textit{object}
```

# **Description**

```
Plot a "scrub_projection" object
```

# Usage

```
## S3 method for class 'scrub_projection'
plot(x, title = NULL, ...)
```

#### **Arguments**

x The "scrub\_projection" object

title (Optional) If provided, will add a title to the plot.

... Additional arguments to ggplot, e.g. main, sub, xlab, ylab, legend.position

#### Value

A ggplot

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pscrub

Projection scrubbing

#### **Description**

Projection scrubbing is a data-driven method for identifying artifact-contaminated volumes in fMRI. It works by identifying component directions in the data likely to represent patterns of burst noise, and then computing a composite measure of outlyingness based on leverage within these directions, at each volume. The projection can be PCA, ICA, or "fused PCA." Projection scrubbing can also be used for other outlier detection tasks involving high-dimensional data.

# Usage

```
pscrub(
  Χ,
  projection = c("ICA", "PCA"),
 nuisance = "DCT4",
  center = TRUE,
  scale = TRUE,
  comps_mean_dt = FALSE,
  comps_var_dt = FALSE,
  PESEL = TRUE,
  kurt_quantile = 0.99,
  get_dirs = FALSE,
  full_PCA = FALSE,
  get_outliers = TRUE,
  cutoff = 4,
  seed = 0,
  ICA_method = c("C", "R"),
  verbose = FALSE
)
```

# **Arguments**

Χ

Wide numeric data matrix (T observations by V variables,  $T \ll V$ ). If X represents an fMRI run, T should be the number of timepoints and V should be the number of vertices/voxels. Projection scrubbing will measure the outlyingness of each row in X.

projection

One of the following: "ICA" (default) or "PCA".

nuisance

Nuisance signals to regress from each column of X. Should be specified as a design matrix: a T by N numeric matrix where N represents the number of nuisance signals. Or can be "DCT4" (default), which will create a matrix with a constant column (the intercept term) and four DCT bases. This default nuisance regression will have the effect of demeaning and detrending the data by removing low-frequency components. To not perform any nuisance regression set this argument to NULL, 0, or FALSE.

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Detrending is highly recommended for time-series data, especially if there are many time points or evolving circumstances affecting the data. Additionally, if kurtosis is being used to select the projection directions, trends can induce positive or negative kurtosis, contaminating the connection between high kurtosis and outlier presence. Detrending should not be used with non-time-series data because the observations are not temporally related.

Additional nuisance regressors can be specified like so: cbind(1, fMRItools::dct\_bases(nrow(x), 4), more\_nuisance).

center, scale

Center the columns of the data by their medians, and scale the columns of the data by their median absolute deviations (MADs)? Default: TRUE. Centering is necessary for computing the projections, so if center is FALSE, the data must already be centered.

Note that centering and scaling occur after nuisance regression, so even if center is FALSE, the data will be centered on the means if the nuisance regression included an intercept term, as it does by default.

comps\_mean\_dt, comps\_var\_dt

Stabilize the mean and variance of each projection component's timecourse prior to computing kurtosis and leverage? These arguments should be TRUE, FALSE (default), or the number of DCT bases to use for detrending (TRUE will use 4). Note that these arguments affect the projection components and not the data itself. Also, if variance-stabilizing but not mean-stabilizing, the components must already be expected to be mean-stabilized, for example if the data was rigorously detrended; otherwise, the results will be invalid.

Slow-moving mean and variance patterns in the components will interfere with the roles of kurtosis and leverage in identifying outliers. While nuisance can be used to detrend the data, this nuisance regression is estimated *non-robustly*, since a robust model takes too long to estimate at each data location. On the other hand, comps\_mean\_dt and comps\_var\_dt can be used to apply a *robust* nuisance regression at each component, since there are much fewer components than original data locations. Thus, even if the data has been detrended with nuisance it may be helpful to detrend the components with comps\_mean\_dt; furthermore, the data nuisance regression does not address the potential existence of variance patterns in the components.

Overall, for fMRI we recommend enabling comps\_mean\_dt and comps\_var\_dt unless the data has been cleaned not only with a low-pass filter like DCT nuisance regression, but also with anatomical CompCor, ICA-FIX, or a similar data-driven strategy that takes into account common sources of artifactual mean and variance trends such as motion and physiological cycles.

**PESEL** 

Use pesel to select the number of components? Default: TRUE. Otherwise, use the number of principal components with above-average variance.

kurt\_quantile

What quantile cutoff should be used to select the components? Default: 0.99. Use 0 to select all high-variance components regardless of kurtosis value.

We model each component as a length T vector of Normal iid random variables, for which the distribution of kurtosis values can be approximated. The quantile is estimated based on this distribution.

get\_dirs

Should the projection directions be returned? This is the V matrix in PCA and S

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matrix in ICA. The default is FALSE to save memory. However, get\_dirs==TRUE

is required for artifact\_images.

full\_PCA Only applies to the PCA projection. Return the full SVD? Default: FALSE (re-

turn only the high-variance components).

get\_outliers Should outliers be flagged based on cutoff? Default: TRUE.

cutoff Median leverage cutoff value. Default: 4.

seed Set a seed right before the call to pesel::pesel or ica::icaimax? If NULL, do

not set a seed. If numeric (default: 0), will use as the seed.

ICA\_method The method argument to fastICA: "C" to use C code with BLAS (default), or

"R" to use R code.

verbose Should occasional updates be printed? Default: FALSE.

#### **Details**

Refer to the projection scrubbing vignette for a demonstration and an outline of the algorithm: vignette("projection\_scrubbing", package="fMRIscrub")

#### Value

A "pscrub" object, i.e. a list with components

measure A numeric vector of leverage values.

outlier\_cutoff The numeric outlier cutoff value (cutoff times the median leverage).

**outlier\_flag** A logical vector where TRUE indicates where leverage exceeds the cutoff, signaling suspected outlier presence.

**mask** A length P numeric vector corresponding to the data locations in X. Each value indicates whether the location was masked:

- **0** The data location was not masked out.
- -1 The data location was masked out, because it had at least one NA or NaN value.
- -2 The data location was masked out, because it was constant.

**PCA** This will be a list with components:

**U** The T by Q PC score matrix.

**D** The standard deviation of each PC.

**V** The *P* by *Q* PC directions matrix. Included only if get\_dirs.

**highkurt** The length Q logical vector indicating scores of high kurtosis.

U\_dt Detrended components of U. Included only if components were mean- or variancedetrended.

highkurt The length Q logical vector indicating detrended scores of high kurtosis.

nPCs\_PESEL The number of PCs selected by PESEL.

**nPCs** avgvar The number of above-average variance PCs.

where Q is the number of PCs selected by PESEL or of above-average variance (or the greater of the two if both were used). If PCA was not used, all entries except nPCs\_PESEL and/or nPCs\_avgvar will not be included, depending on which method(s) was used to select the number of PCs.

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**ICA** If ICA was used, this will be a list with components:

 ${f S}$  The P by Q source signals matrix. Included only if  ${f get\_dirs}$ 

**M** The T by Q mixing matrix.

**highkurt** The length Q logical vector indicating mixing scores of high kurtosis.

 $M_dt$  Detrended components of M. Included only if components were mean- or variance-detrended.

**highkurt** The length Q logical vector indicating detrended mixing scores of high kurtosis. Included only if components were mean- or variance-detrended.

#### References

- Mejia, A. F., Nebel, M. B., Eloyan, A., Caffo, B. & Lindquist, M. A. PCA leverage: outlier detection for high-dimensional functional magnetic resonance imaging data. Biostatistics 18, 521-536 (2017).
- Pham, D., McDonald, D., Ding, L., Nebel, M. B. & Mejia, A. Less is more: balancing noise reduction and data retention in fMRI with projection scrubbing. (2022).

# **Examples**

```
library(fastICA)
psx = pscrub(Dat1[seq(70), seq(800,950)], ICA_method="R")
```

robdist

Robust distance scrubbing

# **Description**

Scrubbing with robust distance.

```
robdist(
    X,
    RD_cutoff = 4,
    RD_quantile = 0.99,
    trans = c("none", "robust-YJ", "SHASH"),
    bootstrap_n = 1000,
    bootstrap_alpha = 0.01,
    projection = c("ICA", "PCA"),
    nuisance = "DCT4",
    center = TRUE,
    scale = TRUE,
    comps_mean_dt = FALSE,
    comps_var_dt = FALSE,
    PESEL = TRUE,
    kurt_quantile = 0.99,
```

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```
get_dirs = FALSE,
full_PCA = FALSE,
get_outliers = TRUE,
cutoff = 4,
seed = 0,
ICA_method = c("C", "R"),
skip_dimred = FALSE,
verbose = FALSE
```

#### **Arguments**

Χ

Wide numeric data matrix (T observations by V variables, T << V). If X represents an fMRI run, T should be the number of timepoints and V should be the number of vertices/voxels. Projection scrubbing will measure the outlyingness of each row in X.

RD\_cutoff

Default: 4.

RD\_quantile

Quantile cutoff...?

trans

Apply a transformation prior to univariate outlier detection? Three options: "none" (default), "robust-YJ", and "SHASH".

bootstrap\_n

Use bootstrapping to estimate the robust distance null distribution? If so, set this to the number of bootstraps. Default: 100. Use 0 (or FALSE), to use an empirical quantile instead.

bootstrap\_alpha

If using bootstrap (bootstrap > 0), this is the level of the bootstrap CI. Default: 0.99.

projection

One of the following: "ICA" (default) or "PCA".

nuisance

Nuisance signals to regress from each column of X. Should be specified as a design matrix: a T by N numeric matrix where N represents the number of nuisance signals. Or can be "DCT4" (default), which will create a matrix with a constant column (the intercept term) and four DCT bases. This default nuisance regression will have the effect of demeaning and detrending the data by removing low-frequency components. To not perform any nuisance regression set this argument to NULL,  $\emptyset$ , or FALSE.

Detrending is highly recommended for time-series data, especially if there are many time points or evolving circumstances affecting the data. Additionally, if kurtosis is being used to select the projection directions, trends can induce positive or negative kurtosis, contaminating the connection between high kurtosis and outlier presence. Detrending should not be used with non-time-series data because the observations are not temporally related.

Additional nuisance regressors can be specified like so: cbind(1, fMRItools::dct\_bases(nrow(x), 4), more\_nuisance).

center, scale

Center the columns of the data by their medians, and scale the columns of the data by their median absolute deviations (MADs)? Default: TRUE. Centering is necessary for computing the projections, so if center is FALSE, the data must already be centered.

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Note that centering and scaling occur after nuisance regression, so even if center is FALSE, the data will be centered on the means if the nuisance regression included an intercept term, as it does by default.

comps\_mean\_dt, comps\_var\_dt

Stabilize the mean and variance of each projection component's timecourse prior to computing kurtosis and leverage? These arguments should be TRUE, FALSE (default), or the number of DCT bases to use for detrending (TRUE will use 4). Note that these arguments affect the projection components and not the data itself. Also, if variance-stabilizing but not mean-stabilizing, the components must already be expected to be mean-stabilized, for example if the data was rigorously detrended; otherwise, the results will be invalid.

Slow-moving mean and variance patterns in the components will interfere with the roles of kurtosis and leverage in identifying outliers. While nuisance can be used to detrend the data, this nuisance regression is estimated *non-robustly*, since a robust model takes too long to estimate at each data location. On the other hand, comps\_mean\_dt and comps\_var\_dt can be used to apply a *robust* nuisance regression at each component, since there are much fewer components than original data locations. Thus, even if the data has been detrended with nuisance it may be helpful to detrend the components with comps\_mean\_dt; furthermore, the data nuisance regression does not address the potential existence of variance patterns in the components.

Overall, for fMRI we recommend enabling comps\_mean\_dt and comps\_var\_dt unless the data has been cleaned not only with a low-pass filter like DCT nuisance regression, but also with anatomical CompCor, ICA-FIX, or a similar data-driven strategy that takes into account common sources of artifactual mean and variance trends such as motion and physiological cycles.

PESEL

Use pesel to select the number of components? Default: TRUE. Otherwise, use the number of principal components with above-average variance.

kurt\_quantile

What quantile cutoff should be used to select the components? Default: 0.99. Use 0 to select all high-variance components regardless of kurtosis value.

We model each component as a length T vector of Normal iid random variables, for which the distribution of kurtosis values can be approximated. The quantile is estimated based on this distribution.

get\_dirs

Should the projection directions be returned? This is the V matrix in PCA and S matrix in ICA. The default is FALSE to save memory. However, get\_dirs==TRUE is required for artifact\_images.

full\_PCA

Only applies to the PCA projection. Return the full SVD? Default: FALSE (return only the high-variance components).

get\_outliers

Should outliers be flagged based on cutoff? Default: TRUE.

cutoff

Median leverage cutoff value. Default: 4.

seed

Set a seed right before the call to pesel::pesel or ica::icaimax? If NULL, do not set a seed. If numeric (default: 0), will use as the seed.

ICA\_method

The method argument to fastICA: "C" to use C code with BLAS (default), or "R" to use R code.

skip\_dimred

Skip dimension reduction? Default: FALSE.

verbose

Should occasional updates be printed? Default: FALSE.

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# Value

```
A "robdist" object, i.e. a list with components

lwr_50 ...

lwr_80 ...

B_quant ...
```

# **Examples**

```
library(fastICA)
rdx = robdist(Dat1[seq(70), seq(800,950)])
```

rob\_stabilize

Stabilize the center and scale of a timeseries robustly

# Description

Stabilize the center and scale of a timeseries using robust regression of DCT bases on the first and second moments.

#### Usage

```
rob_stabilize(
   x,
   center = TRUE,
   scale = TRUE,
   lmrob_method = "MM",
   rescale = TRUE
)
```

# **Arguments**

x The timeseries to stabilize.

center, scale Center and scale? Default: TRUE for both. If scaling but not centering, the data

must already be centered; otherwise, the results will be invalid. Can also be the number of DCT bases to use for robust stabilization of center/scale; TRUE will

use 4.

lmrob\_method The lmrob\_method argument to robustbase::lmrob.

rescale After stabilizing x, re-center and re-scale to the original mean and variance?

Default: TRUE.

#### Value

the timeseries with its center and scale stabilized

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scrub

Data-driven scrubbing

# **Description**

Performs projection scrubbing or DVARS scrubbing, and optionally thresholds to identify artifactual time points.

## Usage

```
scrub(X, method = c("projection", "DVARS"), ...)
```

#### **Arguments**

 $\mathsf{X}$  A T by V numeric matrix representing an fMRI run. There should not be any

missing data (NA or NaN).

method "projection" (default) or "DVARS"

... Additional arguments to the specific scrubbing function: see pscrub or DVARS.

#### Value

A list with components

 $\textbf{measure} \ \ \textbf{A length} \ T \ \text{vector or data.frame with} \ T \ \text{rows, giving the outlyingness measure}(\textbf{s})$ 

**measure\_info** Describes the outlyingness measure(s)

outlier\_cutoff The outlier cutoff value(s).

**outlier\_flag** A length T vector or data.frame with T rows, where TRUE indicates suspected outlier presence.

scrub\_xifti

Scrub fMRI data in CIFTI format

#### **Description**

Performs projection scrubbing or DVARS scrubbing, and optionally thresholds to identify artifactual time points. Requires ciftiTools and the Connectome Workbench.

```
scrub_xifti(
   X,
   method = c("projection", "DVARS"),
   brainstructures = c("left", "right"),
   ...
)
```

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# **Arguments**

X Path to a CIFTI file, or a "xifti" object.

method "projection" or "DVARS"

brainstructures

Character vector indicating which brain structure(s) to use: "left" (left cortical surface), "right" (right cortical surface) and/or "subcortical" (subcortical and cerebellar gray matter). Can also be "all" (obtain all three brain structures).

Default: c("left", "right") (excludes the subcortex).

... Additional arguments to each specific scrubbing function: pscrub or DVARS.

#### Value

A list with components

**measure** A length T vector or data.frame with T rows, giving the outlyingness measure(s)

**measure\_info** Describes the outlyingness measure(s)

**outlier\_cutoff** The outlier cutoff value(s).

 $\begin{tabular}{ll} \textbf{outlier\_flag} & A \ length \ T \ vector \ or \ data. frame \ with \ T \ rows, \ where \ TRUE \ indicates \ suspected \ outlier \ presence. \end{tabular}$ 

SHASH\_out

Robust outlier detection based on SHASH distribution

# **Description**

A robust outlier detection based on modeling the data as coming from a SHASH distribution.

## Usage

```
SHASH_out(x, maxit = 20, out_lim = 3, weight_init = NULL)
```

#### **Arguments**

x The numeric vector in which to detect outliers.

maxit The maximum number of iterations. Default: 10.

out\_lim SD threshold for outlier flagging. Default: 4.

weight\_init Initial weights. Default: NULL (no pre-determined outliers).

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# Value

A "SHASH\_out" object, i.e. a list with components

out\_idx Indices of the detected outliers.

x norm The normalized data.

**SHASH\_coef** Coefficients for the SHASH-to-normal transformation.

indx\_iters TRUE for the detected outliers for each itertation.

last\_iter Last iteration number.

converged Logical indicating whether the convergence criteria was satisfied or not.

# **Examples**

```
x <- rnorm(100) + (seq(100)/200)
x[77] <- 13
SHASH_out(x)</pre>
```

SHASH\_to\_normal

SHASH to normal data transformation

# **Description**

Transform SHASH-distributed data to normal-distributed data.

# Usage

```
SHASH_to_normal(x, mu, sigma, nu, tau, inverse = FALSE)
```

# Arguments

X	Numeric vector of data to transform.
mu	Parameter that modulates the mean of x.
sigma	Parameter that modulates the variance of $x$ . Must be greater than zero. This parameter is on the logarithm scale.
nu	Parameter that modulates the skewness of x.
tau	Parameter that modulates the tailweight of $x$ . Must be greater than zero. This parameter is on the logarithm scale.
inverse	Transform normal data to SHASH instead? Default: FALSE.

#### Value

The transformed data.

```
summary.scrub_DVARS Summarize a "scrub_DVARS" object
```

# **Description**

Summary method for class "scrub\_DVARS"

# Usage

```
## $3 method for class 'scrub_DVARS'
summary(object, ...)
## $3 method for class 'summary.scrub_DVARS'
print(x, ...)
## $3 method for class 'scrub_DVARS'
print(x, ...)
```

# **Arguments**

```
object Object of class "scrub_DVARS".... further arguments passed to or from other methods.x Object of class "scrub_DVARS".
```

#### Value

A plot of the scrubbing results

```
summary.scrub_FD Summarize a "scrub_FD" object
```

# Description

Summary method for class "scrub\_FD"

```
## S3 method for class 'scrub_FD'
summary(object, ...)
## S3 method for class 'summary.scrub_FD'
print(x, ...)
## S3 method for class 'scrub_FD'
print(x, ...)
```

## **Arguments**

```
object Object of class "scrub_FD".... further arguments passed to or from other methods.x Object of class "scrub_FD".
```

#### Value

A plot of the scrubbing results

```
{\it Summarize \ a\ "scrub\_projection"}\ object
```

# Description

Summary method for class "scrub\_projection"

# Usage

```
## S3 method for class 'scrub_projection'
summary(object, ...)
## S3 method for class 'summary.scrub_projection'
print(x, ...)
## S3 method for class 'scrub_projection'
print(x, ...)
```

# **Arguments**

```
object Object of class "scrub_projection".... further arguments passed to or from other methods.x Object of class "scrub_projection".
```

#### Value

A plot of the scrubbing results

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